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Abstract

The encapsulation of drugs into multivesicular liposomes (MVL) offers a novel approach to sustained-release drug delivery.¹ The large size of MVL particles prevents rapid clearance by macrophages and results in the formation of a depot at the site of injection, which causes the drug to release slowly over time. The presence of two transport resistances – the liposomal bilayer and the gel network – is shown to be responsible for the sustained release.

The aim of this work was to prepare multivesicular liposome-encapsulated hydrophobically-modified chitosan gels for drug delivery applications.

Methods

1. Preparation of Multivesicular Liposome (MVL)

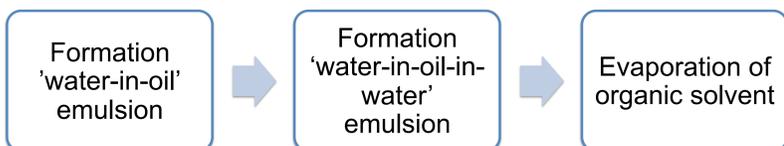


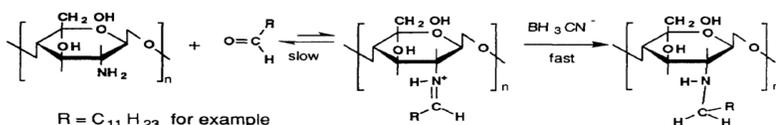
Fig. 1. A schematic image of a multivesicular liposome.



Torrent, Ana. "Exparel" Anesthesia (2012)

2. Synthesis of Hydrophobically-modified chitosan and preparation of MVL-Gel

Hydrophobically modified chitosan was prepared from an alkylation of chitosan.



The hm- chitosan polymer was dissolved in 1% (v/w) acetate solution

The hm-chitosan solution was added drop by drop to MVL solution.

The mixture was left at room temperature for 2 hours before test

Results

Characterization of MVL



Fig. 2. Nikon Eclipse LV100 with Camera System

Fig 3. Optical microscope images of the different steps in the preparation of MVL. A) "water-in-oil" emulsion step, B) "water-in-oil-in-water" emulsion step, C) MVL particles after evaporation of organic solvent.

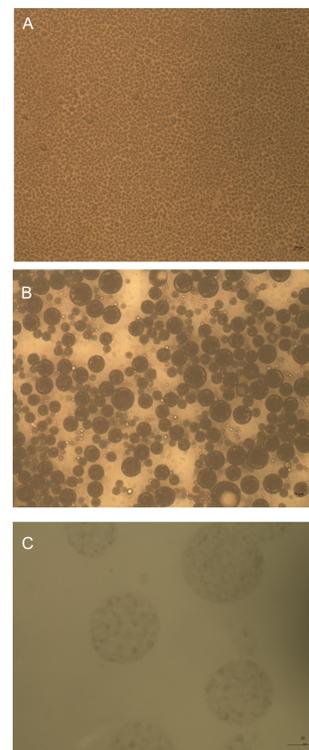


Fig 4. The Tecnai G2 F30 TWIN Transmission Electron Microscope: Displays the size and morphology of the MVL.

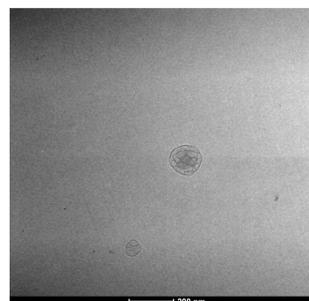
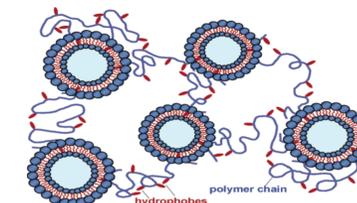


Fig 5. Cryo-TEM Image of MVL



Average particle Size (μm)	Zeta potential (mv)
6	-15.73

Table I. NanoBrook 90Plus Particle Size Analyzer: Determines the size and zeta potential - surface charge - of the MVL.



Lee, Jae-Ho, et al. *Langmuir* 21.1 (2005): 26-33.

Fig 7. Proposed structure of the network formed upon addition of hmc-chitosan to unilamellar liposomes. The hydrophobic part of hmc is shown to be embedded in the bilayer of the liposomes, thus building a connected network of vesicles. Each vesicle acts as a multi-functional cross-link in the network.

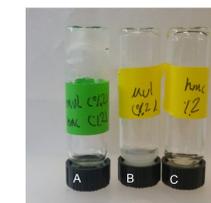


Fig 8. Photograph of (A) 2% hm-chitosan solution+ 2% MVL, (B) 2% MVL and (C) 2% hm-chitosan. At 2 % hm-chitosan, the system is close to the sol-gel transition without the addition of the multivesicular liposome, but it becomes a rigid gel upon the addition of 2% multivesicular liposome with ratio 1:3 (MVL: hmc).

Conclusion

- ❖ The MVLs were obtained by double emulsion process.
- ❖ The characterization of the MVL morphology was through light microscope as seen in Figure 3.
- ❖ Cryo-TEM gives more details of the membrane structure which could be seen in Figure 5.
- ❖ The average particle size is 6μm and the zeta potential is -15.7 mV as listed in Table I.
- ❖ We observe that the 2% hm-chitosan solution is viscous liquid, while contacting 2% hm-chitosan into 2% MVL solution leads to a gel that is able to hold its own weight under vial inversion.

References

1. Mantripragada, Sankaram. "A lipid based depot for sustained release drug delivery" *SkyePharma Inc.* (2002): 393
2. Liu, James, et.al. "Comparison of Sorafenib-Loaded Poly Acid and DPPC Liposome Nanoparticles." *Wiley* (2015):1187-11

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